2003 NMR User Training Course

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Useful Topics for NMR Methodologies

by

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Lecture I:

•Water suppression techniques

Lecture II:

Variant HSQC experiments Pulsed field gradient NMR

Water Suppression Techniques



Sample used throughout this lecture: 1 mM TEP-I in 90% H₂O/10%D₂O, pH 6.0, 290 K.

Water Suppression Technique

- Presaturation
- •Watergate
- •Water flip-back
- •Jump and return, 1-1, 1331
- Suppression by coherence pathway rejection

Water Suppression Technique in Protein NMR



pH Dependence of Amide Proton Exchange Rates

 $N-H + {}^{*}H_{2}O \longrightarrow N-{}^{*}H + {}^{*}H-O-H$



FIGURE 3.26 Intrinsic backbone amide proton exchange rates calculated according to Connelly *et al.* (63). The intrinsic exchange rate, k_{intr} , is shown for exchange of a backbone amide proton with (—) H₂O or (--) D₂O as a function of pH or pD. The pD values are corrected for isotope effects; uncorrected pH meter readings would be 0.4 units smaller.

Figure modified from p154 of John Cavanagh et al., "Protein NMR Spectroscopy: Principles and Practice", Academic Press (1995)

In practice: the pH value for a protein sample for NMR studies is kept below 7.5 to avoid fast exchange rates.



Parameter adjustment: Pulprog=zgpr Adjustment: pl9; power level for presaturation



•A field-gradient pulse is a pulse or a period during which the magnetic field is made deliberately inhomogeneous. $B=B_0+B_g(z)$

•The magnetic field, generated by a gradient pulse, $\rm B_{g}(z)$ varies linearly along the Z-axis

 $B_g(z)=zG_z$, where G_z : gradient strength (G/cm), Z: z-axis position

•Viewing on the rotating frame, spins at different z-position acquire different phase (Larmor frequencies): $\phi(z) = \gamma z G_z \tau$, where ϕ =phase, γ : gyromagnetic ratio, τ : gradient duration

•Actively shielded gradient coil reduces eddy current, and is now popular in multidimensional NMR spectroscopy.



- A. Initially spins in each slice (isochromat) are "phase-coherence".
- B. After a field-gradient pulse, the spins at different slice experience different magnetic field strength, and acquire different Larmor frequencies. The "phase-coherence between slices is now lost due to Larmor precession.
- C. The coherence can be refocused by another gradient pulse (gradient echo).





(figure from p106 of Sattler et al. Prog. In Nucl. Mag. Reson. Spect. 34 (1999)

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WATERGATE







•A strong Z-gradient pulse can be used to destroy transverse magnetization.

•A destroyed (dephased) magnetization can be refocused by another z-gradient pulse of the same amplitude but of opposite phase. (or use a 180 pulse in between the two identical zgradient pulse).

• H_2O : the two extra selective 90 pulse on water makes the 2nd zgradient pulse act as another defocus gradient pulse.

•Protein signals: the 180 pulse makes the 2nd Z-gradient act as a refocus gradient.

Ref: M. Piotto, V. Saudek & V. Sklenar, J. Biomol. NMR 2, 661 - 666 (1992)

WATERGATE



- Parameter adjustment, Pulprog=zgpgwg
- p11: pulse length for 90 degree shaped pulse
- sp1: power level for 90 degree shaped pulse
- spnam1: name of shaped pulse

For example: set spnam1=Sinc1.1000, p11=1 msec, Minimize the water fid by adjusting sp1 in the "gs" utility.

WATERGATE V.S. Presaturation





Sklenar et al., J. Magn. Reson., A102, 241-245 (1993)

- Off resonance DANTE excitation technique.
- 3-9-19: 3α - τ -9 α - τ -19 α - τ -3 α , where 26α =180, τ =delay. (This is also referred as "W3".)



Delay $\tau = 1/(4 \Delta \upsilon_{max})$, where $2\Delta \upsilon_{max}$ =distance of next null (Hz). (The delay τ is field-dependent !!)

3-9-19 WATERGATE

Delay $\tau = 1/(4 \Delta \upsilon_{max})$, where $2 \Delta \upsilon_{max} =$ distance of next null (Hz). (The delay τ is field-dependent !!)

For example: Have the center of NH region (i.e. 8.2 ppm) to be the center of maximal excitation region:

 $\tau = 1/[4^{*}(8.2-4.75)^{*}600.13] = 121$ usec @600 MHz machine $\tau = 1/[4^{*}(8.2-4.75)^{*}500.13] = 145$ usec @500 MHz machine

Parameter adjustment: Pulprog=p3919 Set pl18=pl1, p27=p1, p0=p1 ;d19: delay for binomial water suppression ;d19 = (1/(2*d)), d = distance of next null (in Hz)

Adjust d19 according to the magnetic field strength and where you want the center of maxima excitation to be.



Water Flip-back WATERGATE



S. Grzesiek and A. Bax, J. Am. Chem. Soc., 115, 12593-12594 (1993)

•Water is aligned along the z axis before any z-gradient pulse (point "a"). So, it is not destroyed by the z-gradient pulse.

•This reduces the signal loss of exchangeable protons due to attenuation of water signal (saturation transfer).

Parameter adjustment: Pulprog=*fp*, i.e. "hsqcetfpf3gp" calibrate the shaped pulse as describe in WATERGATE.

Pulse Sequence for Observing Fast-Exchanging Protons

 $N-H + {}^{*}H_{2}O \longrightarrow N-{}^{*}H + {}^{*}H-O-H$

Imino protons in DNA, hydroxyl protons (-OH), Histidine side chain protons in proteins are usually in a fast exchange process with water.

•Flip-back WATERGATE (marginal performance) •Jump and return 1-1

•1-3-3-1

Jump and Return: 1-1



P. Plateau et and M. Gueron, al., J. Am. Chem. Soc. 1982, 104, 7310-7311



- Water signal: "on resonance", aligned to the "z" axis,
- **Protein signals:** free to precess on the transverse plan
- Peak Intensity: $I_x Sin(\Omega \tau)$
- **Delay** $\tau = 1/(4\Delta \upsilon_{max})$, $\Delta \upsilon_{max}$ =distance of maxima intensity
- For example: To observe a peak at 14 ppm at 600 MHz, τ=1/[4*(14-4.75)*600.13]=45 usec

Parameter adjustment: Pulprog=p11

p1: 90 pulse, p0: 90 degree "return" pulse, adjust p0 to be slightly shorter than p1 (0.1-0.3 usec).

d19: d19= (1/(2*d)), d = distance of next null (in Hz)

Binominal: 1-3-3-1



P.J. Hore, J. Magn. Reson., 55, 283-300 (1983)

•Delay $\tau = 1/(2\Delta \upsilon_{max})=1/d$, $\Delta \upsilon_{max}$ =distance of maximal intensity d=distance of next null

•For example: To observe a peak at 14 ppm at 600 MHz, $\tau=1/[2*(14-4.75)*600.13]=90$ usec

Parameter adjustment:

- Pulpro=p1331
- d19: delay for binomial water suppression
- d19 = (1/d), d = distance of next null (in Hz)=2*distance of maximal intensity
- d19=τ as defined above



Jump-Return 1-1 and Binominal 1-3-3-1



Binomial excitation profiles of 1-1 and 1-3-3-1.

John Cavanagh et al., page 154, "Protein NMR Spectroscopy: Principles and Practice", Academic Press (1995)

Jump-Return 1-1 and Binominal 1-3-3-1

Both are for observing fast exchanging protons.

•1-3-3-1: Better water suppression (higher receiver gain), but with offset-dependent phase distortion

•1-1: low receiver gain, the dispersive tail of water interferes with the signals of interest.



What are you trying to detect ?





Water Suppression via Coherence Pathway Rejection

Coherence pathway selected by gradients:

In a gradient selection experiment (echo/antiecho), the water coherence is not "refocused" by the refocus gradient (therefore, is not selected), this naturally suppression the water signal.

Example: cosydfetgp.1, hsqcetf3gp



field gradients



Figure from John Cavanagh et al., "Protein NMR Spectroscopy: Principles and Practice", Academic Press (1995)

Practical Implementation: 1D, 2D and 3D

Fast exchangeable proton (His sidechain, -OH): 1-1 (good for 2D), 1-3-3-1 (not suitable for 2D, 3D).

Exchangeable NH: Water-flip-back HSQC, Fast-HSQC.

Signals (H_{α}) near water: (i.e. TOCSY, COSY) WATERGATE with selective pulse, echo-antiecho PFG.

Variant HSQC Experiments

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Coherence Order

- Zero quantum coherence: I_zS_z...etc
- Single quantum coherence: $I_x S_{z_1} I_y S_{z_2} I_z S_y$... etc
- Double quantum coherence: $I_x S_{x, j} I_x S_{y, j}$...etc
- Triple quantum coherence: $I_x K_x S_{x,j} I_x K_x S_y$... etc
- **HSQC**: Hetero-nuclear single quantum coherence.
- HMQC:Hetero-nuclear multiple quantum coherence.

Scalar Coupling (J-Coupling)



•Scalar couplings (J-couplings) are used as basic magnetization transfer in correlation spectroscopy.

•The efficiency of transfer depends on the magnitude of Jcoupling constants.

HMQC VS HSQC

- HMQC:Hetero-nuclear multiple quantum coherence. Schem a.
- $2\tau = 2*(1/4*J_{IS})$
- N-H: 2*[1/(4*90)]=5.5 ms
- C-H: **2***[1/(4*140)]=**3.6** ms

- HSQC: Hetero-nuclear single quantum coherence. Scheme b. •Intensity: $2I_zS_ysin(2\pi J_{IS}t)$. Maximal intensity with t=1/4J_{IS}
- $\tau = 1/4 * J_{IS}$
- N-H: 1/(4*90)=2.7 ms
- C-H: 1/(4*140)=1.8 ms



HSQC: Adjustment of J-Evolution Time



Page 412, John Cavanagh et al., "Protein NMR Spectroscopy: Principles and Practice", Academic Press (1995)

τ=(1/4J_{IS})



To compensate for relaxation loss, adjust the length of delay according to correlation time (i.e. molecular weight) of your proteins.

Constant-Time HSQC



Page 412, John Cavanagh et al., "Protein NMR Spectroscopy: Principles and Practice", Academic Press (1995)

Spectral resolution can be compromised by passive J-coupling.
The resolution of a ¹H, ¹³C correlation (i.e. HSQC) can be enhanced by removing the passive C-C J-coupling (35 Hz) using a "constant time" scheme.

Resolution Enhancement by the Constant Time Scheme



Page 439, John Cavanagh et al., "Protein NMR Spectroscopy: Principles and Practice", Academic Press (1995)

Sensitivity Improvement in HSQC



HSQC Only either $2I_xS_y$ or $2I_zS_x$ is refocused. Pulprog=hsqcf3ph

PEP-HSQC

(PEP: preservation of equivalent pathway) Both $2I_xS_y$ and $2I_zS_x$ are refocused. (2)^{1/2} increase in sensitivity without considering relaxation



Page 441 of John Cavanagh et al., page 154, "Protein NMR Spectroscopy: Principles and Practice", Academic Press (1995)

HSQC With Different Water Suppression Schemes



Water is kept along the Z-axis in both B and C before the final dephasing sequence to avoid saturation transfer.

Figures from Mori et al., J. Mag. Reson. B 108, 94-98 (1995)

HSQC With Different Water Suppression Schemes



Series of 1D HSQC spectra for 10 mM ¹⁵N-N-acetylalanine (pH 9.2) with different recycling delay.

Figures from Mori et al., J. Mag. Reson. B 108, 94-98 (1995)

Practical Usage of Experiments Containing HSQC

•Saturation Transfer: avoid saturating water signal, especially at neutral pH.

•Relaxation: Extra pulse sequence length in "sensitivity enhanced" HSQC can cause sensitivity loss due to T_2 relaxation. This is particularly serious for large proteins (>20 kDa).

Transverse Relaxation-Optimized Spectroscopy (TROSY)

- Constructive canceling of transverse relaxation caused by chemical shift anisotropy (CSA) and by dipole-dipole coupling at high magnetic field.
- Each of the four multiplet components of ¹⁵N-¹H correlation components has different relaxation rates (line width).
- Select only the narrowest component (1 out of 4).

TROSY at 750 MHz



Pervushin et al. v94, p12366,1997 PNAS USA

The Resolution Power of TROSY



Wider and Wuthrich, Current Opinion in Structural Biology, 1999, 9:594-601

TROSY Effect is Field-Dependent



Optimal field strength: 1 GHz for NH; 600 MHz for aromatic moieties (500-800 MHz).

Wider and Wuthrich, Current Opinion in Structural Biology, 1999, 9:594-601

TROSY

Pulprog=trosyf3gpph19, trosyf3gpphsi19

TROSY-HSQC

HSQC



Wider and Wuthrich, Current Opinion in Structural Biology, 1999, 9:594-601

Some Notes on TROSY

- Intrinsic sensitivity loss by just selecting ¼ component.
 (worth doing it when T₂ relaxation is fast for large proteins).
- At the present time, at least 8-step of phase cycling is required to achieve coherence pathway selection.
- TROSY effect is field strength-dependent. Optimal field strength: 1 GHz for NH; 600 MHz for aromatic moieties (500-800 MHz).
- TROSY effect is well suited for large molecule.

"NMR analysis of a 900K GroEL-GroES complex." Flaux et al., Nature V. 418, 11, p207 (2003)

•Solvent suppression.

•Artifact suppression.

Have the coherence of interested align along the z-axis, then destroy any unwanted signals left on the transverse plan.

•Coherence pathway selection.

Select coherence pathway of interested in one single scan instead of 8 or 16 as in phase cycling. More number of increments can be used in 3D, 4D experiment: higher resolution.

•Diffusion measurement to study aggregation.

Pulsed Field Gradient

Bg

Z=0

-B_g

•A field-gradient pulse is a pulse or a period during which the magnetic field is made deliberately inhomogeneous. $B=B_0+B_g(z)$

•The magnetic field, generated by a gradient pulse, Bg(z) varies linearly along the Z-axis

B_g(z)=zG_z, where G_z: gradient strength (G/cm), Z: z-axis position

Viewing on the rotating frame, spins at different z-position acquire different phase (Larmor frequencies):
 φ(z)=γzG_zt,
 where γ: gyromagnetic ratio, τ: gradient duration

A coherence can be dephased by a strong pulse field gradient.
A dephased coherence can be refocused by a refocus-gradient providing the "overall phase change " is zero.

- $\phi_i \text{+} \phi_f \text{=} 0$;Coherence refocused.
- $\phi_i \text{+} \phi_f \neq 0$;Coherence dephased.



(figure from p106 of Sattler et al. Prog. In Nucl. Mag. Reson. Spect. 34 (1999)

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Coherence Pathway Pathway Selection by PFG

 $\Phi_i = G_i P_i \gamma_i$ (phase acquired after the first gradient) $\Phi_f = G_f P_f \gamma_f$ (phase acquired after the second gradient)

 $G_i = s_i B_g \tau_i$ (gradient term) P_i : coherence order, γ :gyromagnetic ratio τ_i :gradient pulse length, S_i : shape factor of a gradient pulse (what kind of shaped pulse).

Coherence Selection by Gradient:		t 2t field gradients
If $\Phi_i + \Phi_f = 0$;Coherence is refocused (selected). (gradient echo)	+2
lf Φ _i + Φ _f ≠ 0	;Coherence is dephased (rejected).	-1

Example: Selection of the coherence pathway p=2 to p=-1 by PFG. $\Phi_i=1*2*1+2*(-1)*1=0$

Figure from Page 225 of John Cavanagh et al., page 154, "Protein NMR Spectroscopy: Principles and Practice", Academic Press (1995)

PFG-NMR: Coherence Selection, Artifact Suppression





FIG. 1. Examples of different applications of pulsed field gradients in heteronuclear NMR. (a) Selection of an $I_z S_z$ intermediate, (b) selection of transverse S-spin magnetization which is being refocused by a 180° pulse, and (c) elimination of transverse S-spin components caused by an imperfect 180° (S) decoupling pulse.

$$I_x S_z \xrightarrow{90_y^\circ(I)} - I_z S_z \xrightarrow{90_y^\circ(S)} - I_z S_x.$$
 [1a]

Unwanted magnetization is associated with terms such as

$$I_y S_z \xrightarrow{90_y^{\circ}(I)} (I_y S_z) \xrightarrow{90_y^{\circ}(S)} I_y S_x$$
 [1b]

$$I_{y} \xrightarrow{90^{\circ}_{y}(I)} I_{y} \xrightarrow{90^{\circ}_{y}(S)} I_{y} \qquad [1c]$$

or

$$I_x \xrightarrow{90_y^{\circ}(I)} - I_z \xrightarrow{90_y^{\circ}(S)} - I_z.$$
 [1d]

Example "a": Destroy the "unwanted" components with a Z-gradient pulse when they are on the transverse plan and the component of interest is a long the z-axis.

A. Bax & S. Pochapsky, J. Magn. Reson. 99, 638-643 (1992)



 $D_s = kT/6\pi\eta r_s$ r_s : hydrodynamic radius

Different size of molecules have different self-diffusion coefficients D_s.

$I_{(2\tau)} = I_0 * \exp[-(\gamma \delta G)^2 (\Delta - \delta/3) D_s]$

γ: gyromagnetic ratio; δ: gradient duration; G: gradient strength, Δ: time between gradient pulse, I_0 : signal intensity in the absence of gradient

Monitor signal intensity as a function of either gradient duration or gradient strength. D_s can then be obtained by nonlinear-squares fits to the above equation.